OREGON HEALTH & SCIENCE UNIVERSITY

SCHOOL OF MEDICINE GRADUATE STUDIES

SUBTYPING COGNITIVE PROFILES IN AUTISM SPECTRUM DISORDER USING A FUNCTIONAL RANDOM FOREST

Ву

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Abstract

DSM-5 Autism Spectrum Disorder (ASD) comprises a set of neurodevelopmental disorders characterized by deficits in social communication and interaction and repetitive behaviors or restricted interests, and may both affect and be affected by multiple cognitive mechanisms. This study attempts to identify and characterize cognitive subtypes within the ASD population using a random forest (RF) machine learning classification model. We trained our model on measures from seven tasks that reflect multiple levels of information processing. 47 ASD diagnosed and 58 typically developing (TD) children between the ages of 9 and 13 participated in this study. Our RF model was 72.7% accurate, with 80.7% specificity and 63.1% sensitivity. Using the RF model, we measured the proximity of each subject to every other subject, generating a distance matrix between participants. This matrix was then used in a community detection algorithm to identify subgroups within the ASD and TD groups, revealing 3 ASD and 4 TD putative subgroups with unique behavioral profiles. We then examined differences in functional brain systems between diagnostic groups and putative subgroups using resting-state functional connectivity magnetic resonance imaging (rsfcMRI). Chi-square tests revealed a significantly greater number of between group differences (p < .05) within the cingulo-opercular, visual, and default systems as well as differences in inter-system connections in the somato-motor, dorsal attention, and subcortical systems. Many of these differences were primarily driven by specific subgroups suggesting that our method could potentially parse the variation in brain mechanisms affected by ASD.

Main Section

Chapter 1: Introduction

Issues in diagnosing and treating ASD

Lack of precision medicine in ASD

Autism Spectrum Disorders (ASD) comprise altered social interactions and/or communication, as well as the presence of stereotyped or repetitive behavior (1). The prevalence of ASD in the global population has been estimated around 1%, but that number has been growing over the past decade (2,3). The variability in symptoms, severity, and adaptive behavior impairment within the ASD population (4) complicates the development of effective treatments and improved diagnostic measures. Such variation also suggests the possibility of discrete ASD subphenotypes and is consistent with the evidence that ASD may encompass multiple etiologies (1,5). Therefore, identifying and differentiating subgroups in this population should help refine ASD diagnostic criteria and further the study of precision medicine for individuals with ASD.

Heterogeneity in ASD

The etiology of ASD is complex, and the ASD diagnosis has been related to multiple cognitive, sensory, and motor faculties (6). We focused here on the cognitive domain. A thorough review of cognitive mechanisms underlying ASD suggested that non-social cognitive mechanisms, including reward, executive function, attention, visual and auditory processing, may affect the presentation of social behavior regardless of specific impairment or the existence of domain-specific social cognitive mechanisms(7). We examined seven cognitive domains related to information processing and control that have varying levels of association with ASD: spatial working memory, response inhibition, temporal discounting of reward, attentional vigilance, facial recognition, facial affect processing and vocal affect processing.

Working Memory

Working memory refers here to a limited capacity cognitive system that retains information in an accessible state which supports human thought processes(8). A vast literature in ASD reveals inconsistent findings as to whether visuospatial working memory may be impaired, suggesting the existence of ASD subgroups, which may drive the observed impairments. Early studies of working memory showed that high (9), but not low (10), functioning children with autism had impairments in verbal and non-verbal working memory. Another found no differences in working memory between children with or without ASD (11). Measures of non-verbal working memory on a non-spatial and non-verbal self-ordered pointing task correlate with visuospatial memory in children with ASD but not children with ASD (12). In contrast, children without ASD, but not children with ASD, show a relationship between language ability and verbal working memory (12). Such heterogeneity may reflect differences in how individuals with ASD may utilize language to augment verbal working memory (13).

More recent studies have supported the hypothesis that children with ASD may use different cognitive mechanisms to support working memory. A large-scale study revealed that children with ASD exhibited

lower performance than unaffected children on a spatial span task (14), requiring children to repeat a sequence of fixed spatial locations indicated by a series of changing colors. Interestingly, the ASD participants had significantly lower verbal, but not performance, IQ. This study is consistent with findings from two recent studies on children with ASD (15,16), one of which showed that better performance on working memory tasks predicted faster development of play behavior (15). However, another recent study found no differences in a similar spatial span task (17). Taken together, all of these findings suggest working memory differences between children with and without ASD are inconsistent, and may be affected by sample differences that comprise different ASD subgroups.

Response Inhibition

Response inhibition refers here to the ability to inhibit a prepotent response, a lower level component of executive function(18). Over 40 studies have examined whether response inhibition is different between individuals with and without ASD (19). While a number of these studies are underpowered, several use large sample sizes and previously validated psychophysical tests. The results from these studies are quite variable, despite large sample sizes and similar task designs. For example, Guerts and colleagues used a stop task to compare stop signal reaction times between TD and ASD children and found a large effect of diagnosis (20), while a more recent study employing the same task found only a small effect of ASD when examining commission errors (21). Although sampling variation may explain divergent results, an interesting possibility is that heterogeneity in ASD helps explain the inconsistency across the literature (19).

Temporal Discounting of Reward

Temporal discounting refers here to the weakening of the subjective value of a reward due to a delay(22). A few studies (23–25) reveal that those with ASD have altered performance on delayed reward discounting tasks. On average, people naturally prefer immediate to delayed rewards of similar values. Different types of rewards may be discounted differently, and may reflect varying preferences for rewards associated with goal-oriented behavior. For example, individuals with ASD discount monetary and social rewards similarly, whereas typically developing (TD) individuals discount social rewards more than monetary rewards (24). ASD individuals may also discount monetary rewards more steeply with respect to time than TD individuals (25).

Attentional Vigilance

Attentional vigilance refers to the ability to maintain an alert state in the absence of an alerting stimulus. It is often measured using continuous performance tasks (CPTs). ASD performance on CPTs show mixed results. An early study found no difference between children with and without ASD on CPT performance. However, the task used long displays and the parameters of the task were not shifted throughout (26). A more recent study using the same version of the task also failed to find differences between children with and without an ASD. However, they did find differences in EEG signals that are important for sustained and selective attention (27), suggesting that individuals with ASD may use an alternative, perhaps compensatory, strategy to perform similarly on CPTs. Consistent with this hypothesis, individuals with ASD show impaired performance on CPTs where the ratio of distractors to targets (28) or inter-stimulus interval (29) varies over the task duration. On the other hand, increasing attentional demands by crowding the visual display does not seem to affect performance in participants with ASD (30).

Processing of facial features, vocal affect, and facial emotion

Previous work has repeatedly suggested that individuals with ASDs may have trouble processing the arrangements of facial features, which may impair facial identity recognition and the ability to link speech to facial expressions. Individuals with ASD show impairments in searching for the eye region on a face (31). Unlike TD individuals, individuals with ASD are not faster at recognizing a part of the face when it is placed in the context of a whole face (32), and performance on facial identity recognition is not maintained when the orientation of a face is altered (33). Impairments in face processing may affect other domains; individuals with an ASD have difficulty integrating visual facial and auditory speech information (34) and do not use visual information from the mouth to guide speech perception (35).

However, results on facial emotion recognition are more mixed (36). Earlier studies found wide variation in facial emotion recognition performance in adults with an ASD (37,38). More recent studies have shown that facial recognition can be improved in ASD, but that this improvement may not generalize when recognizing emotions from faces (39). ASD participants trained to recognize basic emotions like 'happy' or 'sad' for a particular set of identities did not improve recognition on faces from novel identities. Furthermore, ASD participants did not improve at recognizing emotion when the eyes were presented in the context of a whole face, suggesting that such training did not enable individuals with ASD to process the eyes holistically (39).

In summary, multiple information processing streams may be affected in individuals with ASD, but the types of impairment may be heterogeneous within the ASD population, with different individuals showing varying patterns of difficulty. Critically, it is difficult to disentangle from these studies whether individuals with an ASD diagnosis comprise distinct subgroups, as shown by working memory and response inhibition findings. Therefore, it is critical to test whether ASD is heterogeneous categorically and/or multi-dimensionally. The identification of distinct ASD subgroups may enable better mapping of the cognitive domains affected by and/or responsible for ASD.

Lack of clear biomarkers in ASD

Due to the wide variation in behavioral measures related to ASD, many studies have sought brain-based biological markers to identify a common etiology across individuals with ASD. Markers that are measurable via MRI are highly desirable, because they may represent potential targets for diagnostic tools and or treatments. Unfortunately, the results of these studies are varied due to differences in both study design and sample composition.

Structural brain biomarkers indicating heterogeneity

Reviews of structural MRI findings in ASD have found a wide range of putative biomarkers across independent studies (40–42). Whole brain-volume (43) developmental trajectories may differ between individuals with and without ASD. Regionally, the temporal-parietal junction (44), anterior insula (44,45), posterior cingulate (46,47), lateral and medial prefrontal (46), corpus-callosum (48), intra-parietal sulcus (45,49), and occipital cortex (47), have all been shown to be different between samples with and without ASD. This has led a number of reviewers to suggest that the heterogeneity within the disorder may account for the divergent findings (40,41). Indeed, an interesting study by Christine Nordahl in 2007 examined differences between individuals diagnosed with high-functioning autism, Asperger's, and low functioning autism. Compared to TD individuals, these three samples showed varying cortical folding signatures, indicating that the mechanisms underlying the diagnosis for these samples may differ (45).

Functional brain biomarkers indicating heterogeneity

Studies of functional brain biomarkers for ASD have largely centered on studies of resting state functional connectivity MRI (rsfcMRI) for two reasons. First, the hemodynamic response in ASD children has been shown to be largely similar to the hemodynamic response in TD children (50), suggesting that differences in functional MRI reflect differences in neural activity. Second, the absence of a task enables one to examine differences across multiple brain regions and/or networks, similar to structural MRI.

Unfortunately, findings from rsfcMRI have also varied considerably from study to study. Studies have found altered connectivity within the dorsal attention network (51); default mode-network (DEF; (52)); whole-brain (53,54) and subcortical-cortical (55) underconnectivity; whole-brain (56) and cortical-subcortical (57) hyperconnectivity; and altered connectivity within a discrete set of regions dubbed the "social brain" (58). Some studies (59,60) found no differences in functional connectivity. All of these studies differ not only in MRI processing strategies, but also in the diagnostic inclusion/exclusion criteria. More recent studies (51,58,59) also examined differences in processing strategy, but continued to show discrepant results. Taken together, the findings strongly suggest that ASD heterogeneity may limit the replicability of findings.

Chapter 2: Background

Machine Learning approaches in classifying ASD

Machine learning algorithms provide data-driven methods that can characterize ASD heterogeneity by identifying data-driven subgroups of individuals with ASD. However, most studies using machinelearning algorithms focused only on the identification of individuals with ASD, despite recent studies demonstrating moderate success using such algorithms. A large number of studies have tested whether imaging biomarkers can classify whether an individual has or does not have ASD. Early studies had small sample sizes under 100 individuals and showed high classification rates ranging from 80 to 97 percent accurate (61–64). Larger scale studies greater than 100 individuals typically showed modest accuracy in range of 60 to 80 percent (65–67). The discrepancies may indicate poor control of motion in some cases or over-fit models in others(68). Alternatively, the discrepancies might be the result of ASD heterogeneity. Along these latter lines, one of the best classifications of ASD was performed using Random Forests (RF; (67)). RFs are random ensembles of independently grown decision trees, where each decision tree votes as a weak classifier, and classification into the same group can occur through different pathways. ASD classification was improved when behavioral features were incorporated into models, suggesting that ASD may be stratified by differences in brain function and behavior (65). Interestingly, random forests can also enable the identification of subgroups (69), however, to our knowledge no machine learning approach has attempted to do so for individuals diagnosed with ASD.

Novel use of Random Forest (RF) in identifying subgroups within sample

Here we implement a novel approach for using RFs to identify more homogenous ASD subgroups. RFs is a random ensemble classification approach that iteratively grows decision trees to classify data. The RF model produces a proximity matrix that indicates the similarity between participants. This proximity matrix illustrates how often a pair of subjects were grouped into the same terminal node of each decision tree within the RF and is similar to a correlation matrix. Conceptually, we can recast the proximity matrix as a graph, and a community detection algorithm (70) can be used to identify putative subgroups. Several recent studies have used community detection to characterize subpopulations (71). However, one limitation from the approach as it is currently being used is that the community detection approach does not tie the sub-grouping to the outcome measurement of interest. In other words, prior studies have not evaluated whether the similarity measured between participants, which drives the community detection, is associated with the clinical diagnosis. Thus, an approach that ties the defined sub-populations to the clinical diagnosis is better equipped to identify clinically relevant subgroups. We posit that the combination of random forest classification and community detection can assist with this goal.

In the current report we classify children with and without ASD using several information processing and control measures. To attempt to validate the group assignments identified from the cognitive measures, we then compared the strength of rsfcMRI connections, within or between neural systems, across the identified subgroups. Such a link would provide external evidence that these subgroups differ in functional brain organization as it pertains to an ASD diagnosis.

Chapter 3: Materials and Methods

Participants/Demographics

Participants

The study sample consisted of 105 children between the ages of 9 and 13. Age demographics are shown

Age				
Average for All Tests:	TD = 58, A	SD = 47		
TD M (SD) ASD M (SD)	Tstat	p-value		
10.29 (1.48) 12.15 (2.16)	5.237	0.006		
Facial&Affect Processing	g: TD = 55	, ASD = 46		
11.26 (1.51) 12.51 (2.14)	3.426	<.001		
Delay Discounting : T	D = 58, AS	SD =47		
10.12 (1.74) 12.41 (2.50)	5.509	<.001		
Stop Task: TD = 5	8, ASD =	46		
9.91 (1.62) 12.00 (2.29)	5.46	<.001		
Spatial Span Task: TI	D = 58, AS	D = 47		
10.08 (1.69) 11.89 (2.27)	4.69	<.001		
CPT: TD = 58, /	ASD = 47			
9.91 (1.62) 12.07 (2.24)	5.64	<.001		
MRI Data: TD = 4	2, ASD = :	26		
10.73 (1.74) 12.73 (2.03)	5.08	<.001		

Table 1. Age table for ASD and TD samples per test. TD = Typically Developing; ASD = Autism Spectrum Disorder; M = mean; SD = Standard Deviation. Independent-sample ttests revealed that subgroups were significantly differed in terms of age on the Facial and Affect Processing Tasks, Spatial Span, Delay Discounting, CPT, Stop Task, and MRI scans. Note that the demographics for the Facial and Affect Processing Tasks applies to the Face Identity Recognition, Facial Affect Matching, and the Vocal Affect Recognition tasks. in Table 1, PDS in Table S1, and all other demographics are shown in Table 2. The ASD group was recruited by community outreach and referrals from a nearby autism treatment center and included 47 children (11 females) with a mean age of 12.15 years (SD = 2.12) across all tests. All ASD children had their diagnosis confirmed (using DSM-IV criteria) by a diagnostic team that included two licensed psychologists and a child psychiatrist, and were assessed with a research reliable Autism Diagnostic Observation Schedule Second Edition (ADOS; mean ASD = 12.36, SD = 3.371), Autism Diagnostic Interview-Revised interview (ADI-R) and by the Social Responsiveness Scale Second Edition (SRS; TD mean = 17.8, SD = 10.45; ASD mean = 92.32, SD = 27.02) surveys filled out by parents of the children. The TD group included 58 children (31 females) with a mean age of 10.29 years (SD 2.16) for all tests. A Fisher's exact test indicated that gender was significantly different between the two groups (p = 0.025). It should be noted that the gender difference between our groups is consistent with the fact that males are at increased risk for autism in the general population. Parental pubertal developmental stage (PDS) report was used to assess pubertal stage. The PDS information was acquired once for all participants, but was untied to the tasks or MRI visits, which limits our ability to infer from it. For each MRI and task visit, we

calculated the difference between the date of PDS acquisition and the date the task/MRI was acquired. For each task, any participant that had a PDS within 6 months of the task/MRI visit was included. As a result, the reported subject numbers for the PDS, as linked to the task and MRI, vary. However, we did have a single PDS measure acquired for all participants. Median PDS values were calculated from the observable measures on the PDS (e.g. hair growth or skin changes), measures that did not involve

observation (e.g. whether the parent will discuss puberty with his/her child) were excluded. Unsurprisingly, differences in PDS were strikingly similar to the differences observed in age (see: Table S1). Exclusion criteria for both groups included the presence of seizure disorder, cerebral palsy, pediatric stroke, history of chemotherapy, sensorimotor handicaps, closed head injury, thyroid disorder, schizophrenia, bipolar disorder, current major depressive episode, fetal alcohol syndrome, severe vision impairments, Rett's syndrome, and an IQ below 70. Participants in the TD group were also excluded if diagnosed with attention-deficit hyperactivity disorder. Subjects taking prescribed stimulant medications completed medication washout prior to testing and scanning. Children performed tasks and completed MRI visits following a minimum of five half-life washouts, which ranged from 24 to 48 hours given the preparation. Participants on non-stimulant psychotropic medication (e.g. anxioltyics or anti-depressants) were excluded from this study.

Data collection procedures

ASD participants came in for a screening visit to determine if they qualified for the study. During this

IQ scores		
	TD	ASD
WISC BD (M)	38	40.81
WISC BD (SD)	12.78	13.96
		1.074
p value		0.279
Gender		
Males (N)	27	38
Males (%)	46.55	80.85
Females (N)	31	9
Females (%)	54.45	19.15
Pearson's Chi-square		12.951
p-value		<.001
Ethincity		
	49	39
Non-Hispanic (%)	84.48	82.98
Hispanic (N)	9	8
Hispanic (%)	15.52	17.02
Pearson's Chi-square		0.07
p-value		0.966
Race		
White (N)	51	39
White (%)	87.93	82.98
Black/African American (N)	1	2
Black/African American (%)	1.72	4.26
Asian (N)	4	1
Asian (%)	6.7	2.13
Native Hawaiian/Pacific Islander (N)	0	1
Native Hawaiian/Pacific Islander (%)	0	2.13
Pearson's Chi-square		4.295
		0.368

Table 2. Demographics table for ASD and TD samples per test. WISC BD = Wechsler's Intelligence Scale for Children IV: Block design raw score.

initial visit, informed written consent or assent was obtained from all participants and their parents, consistent with the Oregon Health & Science University institutional review board. Additionally, children completed the ADOS and the Wechsler Intelligence Scale for Children IV (WISC-IV; (72)) block design subtest while parents completed the SRS, ADI-R, and Developmental and Medical History surveys. Participants who qualified for the study came back for a second visit where they completed our Delay Discounting, Spatial Span, CPT, and Stop tasks. All participants also experienced a "mock scanner" to acclimate to the scanner environment and to train themselves to lie still during the procedure. Participants then came in for a third visit where they were scanned. At the fourth visit, participants completed our Face Identity Recognition, Facial Affect Matching, and Vocal Affect Recognition tasks.

Participants in the TD group were recruited from a partner study with similar protocol. During the initial screening visit, participants underwent a diagnostic evaluation based on the Kiddie-Schedule for Affective Disorders and Schizophrenia (KSADS) interview, as well as parent and teacher standardized ratings, which were reviewed by their research diagnostic team. TD participants completed their study visits and tasks in a similar timeline and were recruited for our study during their MRI visit. TD participants were then screened and enrolled in an additional visit in which they

completed the Face Identity Recognition, Facial Affect Matching, and Vocal Affect Recognition tasks.

Most of the participants consented to a longitudinal study where they returned on an annual basis to be reassessed on these same tasks and were re-scanned. For this study, we used data from each participant's earliest time point for each completed task and MRI scan. Per task and scan, a t-test was conducted to test whether the cross-sectional ages were significantly different for that test. In all cases, ASD participants were significantly older than TD participants (all p < 0.05). We controlled for non-verbal intelligence, as measured by the WISC block design, by ensuring that block design scores were not

significantly different between the groups (p = 0.285). We also calculated and tested the difference in visit age for the ASD (mean years = 1.51, s.d. (years) = 1.36) and typical (mean years = 1.14, s.d. (years) = 1.17) samples selected. We found no significant group effects on average visit difference (t(103) = 1.49, p = 0.14).

Behavioral Data						
Task	Variable	TD M (SD)	ASD M (SD)	T Score	p-value	df
Delay Discounting	7-day indifference score	8.16 (1.99)	7.65 (2.9)	1.06	0.29	103
Delay Discounting 90-day indifference score		4.81 (3.03)	4.92 (3.81)	-0.16	0.88	103
Delay Discounting	Natural log of k	-4.48 (1.83)	-4.74 (2.2)	0.64	0.53	94
Delay Discounting	30-day indifference score	6.32 (2.91)	5.89 (3.64)	0.66	0.51	103
Delay Discounting	K-value	0.0521 (0.185)	0.057 (0.14)	0.14	0.89	94
Delay Discounting	180-indiffence score	3.77 (3.1)	4.11 (3.82)	0.50	0.62	103
Delay Discounting	Intial indifference score	9.97 (0.417)	9.89 (0.464)	0.99	0.33	103
Delay Discounting	AUC	0.527 (0.26)	0.543 (0.318)	-0.27	0.79	95
Delay Discounting	Timepoint and Score R2 value	0.682 (0.352)	0.566 (0.39)	1.58	0.12	102
Stop Task	Probablity of Stopping on Stop Trials	51 (3.75)	51.4 (5.28)	-0.53	0.60	102
Stop Task	Stop Signal RT (ms)	253 (72.4)	303 (129)	-2.49	0.01	102
Stop Task	Mean RT on Go Trials (ms)	703 (130)	816 (205)	-3.40	0.00	103
Stop Task	Go Trials Accuracy	95.2 (3.48)	95 (4.63)	0.35	0.73	103
Stop Task	SD Go Trials RT (ms)	199 (59.2)	242 (93.5)	-2.84	0.01	103
СРТ	Bias score Stim Trials	-0.301 (0.133)	-0.317 (0.157)	0.52	0.60	100
СРТ	Dprime Stim Trials	2.69 (0.82)	2.67 (0.866)	0.10	0.92	100
СРТ	Dprime Catch trials	1.21 (0.684)	1.41 (0.828)	-1.36	0.18	100
СРТ	Natural Log of Bias Score Stim Trials	1.6 (0.793)	1.72 (1.05)	-0.67	0.50	100
СРТ	Natural log of Bias Score Catch Trials	-0.12 (1.08)	0.0662 (1.42)	-0.74	0.46	100
СРТ	Bias Score Catch Trials	0.057 (0.73)	-0.0191 (0.525)	0.58	0.56	100
Spatial Span	SS Backwards Number Completed	8.59 (2.31)	8.19 (2.99)	0.75	0.42	103
Spatial Span	SS Backward RT (ms)	1290 (438)	1370 (701)	-0.70	0.48	103
Spatial Span	SS Backward Response Consistency	0.619 (0.105)	0.559 (0.143)	2.46	0.02	103
Spatial Span	SS Backward Span Number Correct	5.41 (1.85)	4.87 (2.51)	1.26	0.21	103
Spatial Span	SS Forward Number Completed	9.34 (2.26)	8.79 (2.95)	1.08	0.28	103
Spatial Span	SS Forward RT (ms)	1170 (348)	1170 (443)	0.10	0.92	103
Spatial Span	SS Forward Response Consistency	0.627 (0.0935)	0.622 (0.123)	0.24	0.81	103
Spatial Span	SS Forward Span Number Correct	5.93 (1.93)	5.66 (2.43)	0.63	0.53	103
Facial Affect	Total Correct	18.4 (2.27)	17.1 (3.24)	2.39	0.02	98
Facial Affect	Median RT (s)	5.06 (1.74)	5.45 (1.92)	-1.07	0.29	98
Facial Recogniton	Total Correct	22.6 (1.91)	19.6 (4.06)	4.77	0.00	98
Facial Recogniton	Median RT (s)	6.05 (2.37)	6.22 (3.05)	-0.31	0.76	98
Vocal Affect	Total Correct	16.7 (2.17)	15.8 (3.02)	1.63	0.11	98
Vocal Affect	Median RT (s)	1.96 (0.658)	1.68 (0.72)	2.04	0.04	98

Table 3. Table of task measures used in RF analysis. Independent samples ttests were conducted between all available ASD and TD data. RT = reaction time.

Tasks

Measures derived from seven tasks were used as input features for the random forest. These seven tasks cover multiple levels of information processing, which may affect or be affected by the presence of an ASD diagnosis. Per measure, an independent samples, twotailed, t-test was conducted to evaluate whether ASD and TD participants differed significantly. Table 3 lists each feature along with the t-statistic and pvalue associated with the test. Because the random forest approach is robust against the presence of non-predictive features(73), our initial feature selection was inclusive. Despite this liberal inclusion, these non-predictive features did not contribute meaningfully to the classification model and thus did not affect results materially (supplementary materials).

Delay Discounting

The Delay Discounting task measures an individual's impulsivity by asking them to evaluate a reward's subjective value following a delay. The task design employed here has been described in detail previously (74,75). In short, this computerized task consisted of 91 questions and requested participants to choose between two hypothetical amounts of money, one smaller amount that would be available immediately, and one larger amount that would be available after a fluctuating delay (between 0 to 180 days). No actual money was obtained. We used 9 variables from this task in our RF model: the indifference score at 5 time points (7, 30, 90, or 180 days), the calculated area under the curve (AUC) based on these indifference scores, the proportion of variance explained between the scores and their timepoints, their k value (a measure of overall rate of discounting), and the natural log-transformation of these k values. Three validity criteria were applied(76): 1) an indifference point for a specific delay could not be greater than the preceding-delay indifference point by more than 20% (\$2); 2) the final (180 day) indifference point was required to be less than the first (0 day) indifference point, indicating evidence of variation in subjective value of rewards across delays; and 3) the 0-day indifference point was required to be at least 9.25. Lower values for the 0-day indifference point indicate that the child chose multiple times to have a smaller reward now over a larger reward now, suggesting

misunderstanding or poor task engagement. Data that did not meet validity criteria were treated as missing in analyses.

Spatial Span

The Spatial Span task measures an individual's visuospatial working memory capacity. Our participants received a spatial span subtest identical to the computerized Cambridge Neuropsychological Test Battery (CANTAB; (77)). Briefly, this computerized task presents a series of 10 white boxes randomly placed on the screen, a subset of which would change color in a fixed order. Participants were instructed to watch for boxes that changed color and to keep track of their sequence. In the spatial forward task, participants were instructed to click on the boxes in the same sequential order in which they were presented. In the spatial backward task, participants were instructed to click on the boxes in the reverse order in which they were presented. The tasks were counterbalanced, and every subject had the opportunity to practice before administration. At the beginning of both tasks, the numbers of squares that changed started at three and increased to nine, with two trials at each sequence length (a total of 24 trials for both tasks). The task discontinued when a child failed both trials at a sequence length. We used 8 measures from this task in our RF model: reaction time, accuracy, number completed, and span number correct for both the forward and backward tasks.

Stop Task

A tracking version of the Logan stop task was administered to all participants(78,79). The Stop Task is a dual go-stop task. The go portion of the task measures reaction time and variability of reaction time on a simple choice detection task; the stop portion measures speed at which the individual can interrupt a prepotent response (how much warning is needed). For this computerized task participants fixated on a small cross in the center of computer screen, which appeared for 500ms on each trial. For the "go trials" (75% of total trials), either a rainbow "X" or an "O" would appear on the screen for 1000ms. Participants then had 2000ms to indicate whether they saw an "X" or an "O" using a key press, after which the next trial would automatically start. The "stop trials" (25% of total trials) were identical except that an auditory tone was played briefly after the presentation of the visual cue. The timing of the tone was varied stochastically to maintain approximately 50% success at stopping. Participants were instructed to not respond with the key press if they heard the tone. Each participant performed 20 practice trials to ensure they understood the task, before completing eight 32 trial blocks of the task. We used 5 measures from this task in our RF forest model: accuracy of the X/O choice on "go-trials", probability of successful stopping on the "stop-trials", stop signal reaction time (computed as the difference between go RT and timing of the stop delay warning signal), mean reaction time on go-trials, and the standard deviation of reaction times during "go-trials".

Continuous Performance Task

The Continuous Performance task was an identical-pairs version of the common CPT, which measures vigilance. For this computerized task participants viewed a series of four digit numbers (250ms per cue) and were instructed to press a button whenever they saw a pair of identical numbers back-to-back. The task consisted of three types of trials: 1) trials where the paired numbers were made of distinct digits called "stim trials", 2) trials where paired numbers only differed by one digit called "catch trials" and 3) trials where the pair of numbers were identical (target trials). The task included a total of 300 stimuli and required about 10 minutes to complete. There were 20% target trials, 20% catch trials, and 60%

"stim" or non-target trials. We used 6 measures from this task in our RF model: dprime (a measure of discriminability(80)) per discrimination type (essentially, "hard" and "easy" discriminations), bias score for each discrimination type, and the natural log of bias per discrimination type.

Face Identity Recognition Task

The Face Identity Recognition Task was designed by the Center for Spoken Language Understanding (CSLU) at OHSU to measure facial processing skills. In this computerized identification task, for each of the 25 trials (inter-trial interval = 2s), participants were presented with a "target face" on the left side of the screen, a colored photograph of a human face presented in standardized poses with neutral facial expressions. At the same time participants were shown an additional four facial photographs on the right side of the screen (all photographs were selected from the Glasgow Unfamiliar Faces Database (81), see Fig 1B), one of which matched the target face. Participants were asked to select the target face out of the lineup by touching the screen with stylus pen. Reaction times were calculated from the moment the trial began to the participant's response; however, participants were not told they were being timed or instructed to complete the task as quickly as possible. Each participant was allowed five practice trials to ensure they understood the task. We used 2 measures from this task in our RF model which included the number of correct responses and the median reaction time for all trials.

Facial Affect Matching Task



Figure 1. Depiction of stimuli used in face and affect processing experiments. (A) Example from visual facial affect recognition task. (B) Example from facial identity recognition task. (C) Example from auditory facial affect recognition task.

The Facial Affect Matching Task and was designed by the CSLU at OHSU to measure affect discrimination skills using facial expressions. In this computerized task, for each of the 25 trials (inter-trial interval = 2s), participants were presented with a "target emotion", a colored photograph of a human face expressing one of six possible emotions (happiness, sadness, surprise, disgust, fear or anger), on the left side of the screen. At the same time participants were shown an additional four facial photographs on the right side of the screen (all photographs were selected from the NimStim set of facial expressions (82), see Fig 1A), one of which matched the target emotion. Participants were asked to select the target emotion out of the lineup by touching the screen with stylus pen. Reaction times were calculated from the moment the trial began to the participant's

response; however, participants were not told they were being timed or instructed to complete the task as quickly as possible. Each participant was allowed five practice trials to ensure they understood the task. We used 2 measures from this task in our RF model which included the number of correct responses and the median reaction time for all trials.

Vocal Affect Recognition

The Affect Matching Task was designed by the CSLU g at OHSU to measure affect discrimination skills using auditory cues. In this computerized task, for each of the 24 trials (inter-trial interval = 2s), participants were presented with an audio recording of an actor reading neutral phrases (e.g., "we leave tomorrow") but expressing one of four possible emotions (happiness, sadness, fear or anger) during the reading. Participants were asked to identify what type of emotion the actor was expressing by selecting one of four black and white drawings of facial expressions, each depicting one of the 4 basic emotions (see Fig 1C). Reaction times were calculated from the moment the trial began to the participant's response; however, participants were not told they were being timed or instructed to complete the task as quickly as possible. Each participant was allowed four practice trials to ensure they understood the task. We used 2 measures from this task in our RF model which included the number of correct responses and the median reaction time for all trials.

MRI scans

Data acquisition

Participants were scanned in a 3.0 T Siemens Magnetom Tim Trio scanner (Siemens Medical Solutions, Erlangen, Germany) with a 12 channel head coil at the Advanced Imaging Research center at Oregon Health and Science University. One T1 weighted structural image (TR = 2300ms, TE = 3.58ms, orientation = sagittal, FOV = 256x256 matrix, voxel resolution = 1mmx1mmx1.1mm slice thickness), and one T2-weighted structural image (TR = 3200ms, TE = 30ms, flip angle= 90° FOV =240mm, slice thickness = 1mm, in-plane resolution = 1 X 1mm) was acquired for each participant. Functional imaging was performed using blood oxygenated level-dependent (BOLD) contrast sensitive gradient echo-planar sequence (TR = 2500ms, TE = 30ms, flip angle = 90°, in-plane resolution 3.8x3.8mm, slice thickness = 3.8mm, 36 slices). For fMRI data acquisition, there were three 5-minute rest scans where participants were asked to relax, lie perfectly still and fixate on a black cross in the center of a white display.

General preprocessing

All functional images went through identical Human Connectome Project preprocessing pipelines as described previously (83) in order to reduce artifacts. These pipelines included 1) PreFreeSurfer, which corrects for MR gradient and bias field distortions, performs T1w and T2w image alignment, and registers structural volume to MNI space; 2) FreeSurfer (84), which segments volumes into predefined cortical and subcortical regions, reconstructs white and pial surfaces, and aligns images to a standard surface template (FreeSurfer's fsaverage); 3) PostFreeSurfer, which converts data to NIFTI and GIFTI formats, down sampled from a 164k to a 32k vertices surface space, applies surface registration to a Conte69 template, and generates a final brain mask. 4) fMRIVolume, which removes spatial distortions, performs motion correction, aligns fMRI data to the subject's structural data, normalizes data to a global mean, and masks the data using the final brain mask, and 5) fMRISurface which maps the volume time series to a standard CIFTI grayordinate space.

Functional connectivity processing

All resting state functional connectivity MRI data received additional preprocessing that have been widely used in the imaging literature (85) to account for signals from non-neuronal processes. These steps included: 1) removal of a central spike caused by MR signal offset, 2) slice timing correction 3) correction for head movement between and across runs, 4) intensity normalization to a whole brain mode value of 1000, 5) temporal band-pass filtering (.009Hz < f <.08 Hz), 6) regression of nuisance variables: 36 motion related parameters, and three averaged signal timecourses from the grayordinates,

white matter, and cerebrospinal fluid (CSF). Additionally, because previous research has indicated that minor head movement can result in changes in MRI signal, we performed motion-targeted "scrubbing" on all rs-fcMRI data (85). These steps included censoring any volumes with frame displacement (FD) > .2mm, and the elimination of any run with less than a total of two and a half minutes of data.

Correlation matrix generation

All timecourses and correlations were derived from a set of 333 Regions of Interest (ROIs) produced from a published data-driven parcellation scheme (Figure 4) (86), and a set of 19 subcortical areas parcellated by FreeSurfer during preprocessing. The resulting parcellations set comprised 352 ROIs. Correlations between ROIs were calculated using Pearson product-moment coefficient between each pair of ROIs over the extracted time series following preprocessing and motion censoring. We created a correlation matrix for each participant and then created group correlation matrices by averaging individual matrices across groups and subgroups.

Data Analysis

Exploratory Data Analysis

Prior to construction of the RF model, we measured the quantity of missing data. Machine-learning model performance can be greatly affected by missing data. Therefore, we excluded any measures and participants that were missing more than 15 percent of data. The remaining missing data is imputed separately for the training and test datasets using the random forest algorithm below, where the missing data's column is the outcome measure and the remaining variables are used as predictors. Prior to our exploratory data analysis we had a total of 143 subjects (73 ASD, 70 TD) with partially completed data, after eliminating subjects with more than 15 percent missing data we finalized our subject list down to 105 (47 ASD, 58 TD). In the final dataset, less than 3 percent of all possible data was missing. An inspection of the missing data was unable to find any patterns that distinguish the missing ASD data from the remaining cases.

Random Forest classification

General algorithm

The RF algorithm constructs a series of decision trees. Per tree, a bootstrapped dataset is generated from a subset of the training data and a subset of features are randomly used to predict group classification or outcome measure in the case of imputation. The Gini impurity is used as the cost function to determine the optimal tree for classification and the mean square error is used as the cost function to determine the optimal tree for regression. Finally, a testing dataset comprising participants that were excluded from the training dataset is used to evaluate classification model performance. We implemented this algorithm via in-house custom-built MATLAB programs that used the MATLAB TreeBagger class. 1000 trees were used for the classification model and 20 trees were used for the surrogate imputation. Missing data was imputed separately for training and testing datasets. For classification, 1000 iterations of the RF algorithm were run to assess the performance of the RF models. Per iteration, 60 percent of participants formed the training dataset.

Optimization and validation

Distributions of overall, ASD, and control accuracy were constructed from the 1000 iterations and compared against a distribution of 1000 null-models. Per null-model, the group assignments are randomly permuted and the RF procedure above is performed on the permuted data. If the RF

classification models are significantly better than the null models, then we interpret the RF models as valid for predicting a given outcome measure. An independent samples t-test was used to evaluate the significance of the RF model performance against the null model performance based on the models' accuracy, specificity, and sensitivity rates.

Community detection

Since each tree has different terminal branches, the RF algorithm may identify different paths for participants with the same diagnosis. Therefore, validated models can be further analyzed to identify putative subgroups that reflect the same diagnosis but perhaps different etiologies. Briefly, the RF algorithm produces a proximity matrix, where the rows and columns reflect the participants and each cell represents the proportion of times, across all trees and forests, a given pair of participants ended in the same terminal branch. For the classification model, the Infomap algorithm (Rosvall, 2007) was used to identify putative subgroups from the proximity matrix for participants with an ASD and from the proximity matrix for control participants. Because we have no basis for determining what constitutes an edge, an iterative procedure was used (87), where we identified a consensus set of community assignments across all possible thresholds.

Radar plot visualization

Task measures were then examined via radar plots to identify features that distinguish putative subgroups. Since plotting all measures may obscure differences between the groups, visualized task measures were chosen via statistical testing. For the ASD and the TD samples separately, one-way ANOVAs, with subgroup as the factor and each subgroup a level, were conducted for each task measure. Significant (p < 0.05) task measures were chosen for visualization. Individual task measures were converted to percentiles and visualized by task.

Functional connectivity cluster analysis

We used a chi-square approach to identify potential differences between subgroups within or between functional systems, as opposed to individual functional connections (88). Briefly, three sets of mass univariate tests were conducted for all Fisher-Z transformed functional connections: a set of one-way ANOVA using ASD subgroup as the factor, a set of one-way ANOVAs using control subgroup as the factor, and a set of t-tests between ASD and control groups. Per set, a matrix of coefficients are extracted and binarized to an uncorrected p < 0.05 threshold. This binary matrix is then divided into modules based on the published community structure (89) which reflects groups of within system (e.g. connections within the default mode system) and between system (e.g. connections between the default mode system and the visual system) functional connections. The subcortical parcellation was defined as its own system for this analysis because of prior research suggesting differences between cortical and subcortical connectivity (55). A ratio of expected significant to non-significant functional connections (i.e. the expected ratio) is calculated by dividing the total number of significant connections by the total number of all connections. Per module, the number of expected significant and nonsignificant functional connections is determined by multiplying the expected ratio by the total number of functional connections within the module. A chi-squared statistic is then calculated using the observed and expected ratio of significant connections. Permutation tests were conducted for all functional connections across the 352 ROIs to calculate the p value per module, and evaluate whether the observed clustering is greater than what would be observed by random chance.

Supplemental analysis 1: Evaluation of age and gender on input features Justification

In our sample, ASD outcomes varied by age and gender, but it is possible that, within our specific sample, such variation may not be associated with performance on the tasks measured. Therefore, we examined whether age and gender were associated with task measures using linear and logistic regression. If age and gender are associated with specific measures, then such measures may not be specific to clinical outcomes, and age and gender could drive RF classification. If age and gender are unrelated to specific measures, then such measures are specific to clinical outcomes, and it is less likely that age and gender drive RF classification.

Approach

In order to evaluate whether age and gender may have driven the results in our main manuscript, we performed a linear regression analysis for age and a logistic regression analysis for gender against the 34 features used as predictors in the random forest (RF) algorithm. All data across ASDs and TDs were used in the regression analysis, in order to assess how much effects of ASD on gender and age may have influenced our primary findings. False Discovery Rate (FDR) with a q of 0.05 was used to correct for multiple comparisons. We assessed the effect size for each regression using R-squared values as the measure of effect size. If R-squared values are low for all features, it would suggest that age and gender are not driving factors in our analysis.

Supplemental analysis 2: RF classification when controlling for age and gender Justification

Supplemental analysis 1 suggested that RF classification may not be affected by associations between task performance and age or gender, but it is far from conclusive. We can further address this question directly by testing whether RF classification accuracy is affected when controlling for age and gender. If RF accuracy is unaffected, then we can be certain that age and gender did not affect RF classification performance. Unfortunately, due to the strong association between age, gender, and clinical outcome, reductions in RF classification performance should be expected, even if age and gender are weakly related to the task performance measures. However, if RF model performance falls below chance, it is more likely that RF classification was driven by demographics. If RF model performance is above chance, subgroups will be identified via Infomap and examined further to explore what features may drive RF classification in this supplemental analysis.

Approach

We controlled for age and gender via linear and logistic regression separately. Per feature, the residuals from linear regression of the feature against age were calculated, and the residuals were input into a logistic regression against age, where new residuals were calculated. This procedure resulted in 34 residual features, controlling for both age and gender, which were used as input for the RF algorithm (see the main manuscript for details). It is important to interpret these results cautiously. Because gender and age are different between ASD and TDs, if gender and age are not related to the predictors, then this regression procedure may add variance into the input data without removing any bias. In other words, because of the gender and age confounds, reduced classifier performance is expected when performing regression.

Supplemental Analysis 3: Effect of subgroup on ADOS scores Justification

The social responsiveness scale (SRS), while a quantitative estimate of autism symptom severity, may fail to capture aspects of autism traits that can be captured through other instruments. In order to further test whether ASD subgroups varied in autism symptom severity measures, we examined whether autism symptom severity, as measured by the Autism Diagnostic Observation Schedule (ADOS), varied between ASD subgroups. The ADOS measures observed child behavior as the child interacts with a trained clinician, while the SRS is a parental report of symptoms over an approximate six month period. Therefore the ADOS represents a very different type of measure than the SRS. If no differences in ADOS symptom severity is observed, we can be more confident that the ASD subgroups reflect typical heterogeneity more than autism symptom severity.

Approach

We used a one-way ANOVA to examine the effect of subgroup on ADOS sum scaled scores, where subgroup was modeled as a factor and the ADOS sum scaled scores were the dependent variable. We performed this analysis for the subgroups identified by both the original (Figure 9A), and supplemental (Figure 9B) analyses.

Supplemental Analysis 4: comparison of demographics between ASD subgroups and between TD subgroups

Justification

Variation in typical heterogeneity could be explained either by cognitive or demographic factors, such as age and gender. Therefore, we examined whether demographic traits like age and gender, or cognitive traits like intelligence vary between the ASD and TD subgroups. Variation in such demographic factors and not autism symptom severity would indicate that RFs were sensitive to demographic factors. Comparing demographic differences between the original and supplemental RF subgroups may indicate how age and gender regression affected subgroup affiliation.

Approach

In order to examine factors that may drive subgroup identification, we examined whether ASD and TD subgroups showed significant variation in gender, age, or intelligence as measured by the WISC-IV block design scaled score. Age per individual was calculated as the mean age across all behavioral tasks the individual participated in. We excluded the MRI ages because those would not factor into the RF model itself, for MRI data were analyzed independently from the RF model. As with ADOS symptom scores, we used separate one-way ANOVAs per age and IQ measure to test the effect of subgroup on ASD and TD subgroups. For gender, we used a chi-squared analysis. Both supplemental and original RF subgroups were examined.

Supplemental Analysis 5: comparison of demographics between accurately classified subgroups Justification

Because it is unclear whether regression produced an RF model that identified artefactual or meaningful subgroups, we tested whether age and IQ varied between accurately classified ASD and TD subgroups. If accurately classified subgroups in the original RF model do not differ by age or IQ, then it is unlikely that the original RF model classified participants on the basis of such factors, suggesting that variation in typical cognitive profile may have driven RF classification and subgroup identification. If accurately classified subgroups in the supplemental RF model differ by age or IQ, then it is likely that the

supplemental RF model classified participants by demographics, suggesting that demographic variation may have driven the supplemental results.

Approach

If RF classification accuracy is driven by variation in demographics, we should expect to see significant differences in age/gender/IQ between the accurately classified subgroups. Therefore, we tested whether the RF classification was driven by demographic variables (i.e. age, gender, and IQ) using one-way ANOVAs and chi-squared tests. Subgroups whose accuracy was greater than random chance were modeled in the analyses. As with the above analyses, we examined both the original and supplemental subgroups, to see how controlling for age and gender via regression impact subgroup composition.

Supplemental Analysis 6: examination of variable importance from features

Justification

Because associations between input features and demographics varied across tasks and measures, we evaluated the importance of each feature used in the original RF. This analysis provides context for the supplemental analyses above. If features important for classification were associated with age and gender, we would anticipate that controlling for age and gender would produce a more appropriate model. On the other hand, if features important for classification are unrelated with age and gender, such regression could contaminate the analysis, because age and gender are associated with the clinical outcome in our sample. Additionally, a number of included features are controlled by the experimenter, and should not be useful in classification. If such features were important for classification, then the RF model may be affected by variation in task parameters, and not task performance.

Approach

Features used in the RF algorithm were assessed for variable importance(73). Briefly, cases not used in the bootstrapped dataset for a given tree, also known as the out of bag (OOB) cases, are run through the decision tree and the OOB error rate is calculated. Per feature, the values for the OOB cases' given feature are then permuted and the difference between the permuted OOB error rate and observed is calculated. This procedure is repeated across all trees, and because each tree is independent, a z-score can be calculated for each feature across all trees. Thus, this variable importance measure indicates which variables meaningfully contribute to classification.

The eight features showing improved classification accuracy were entered into a supervised random forest algorithm, to assess the performance of these eight features vs. including all 34 features across all tasks. Age and gender were not regressed in order to compare the RF performance with the original RF. 1000 iterations were run with 40 percent holdout (see: Supplemental Analysis 2; methods, for more details) for testing data and 60 percent as training data. Mean and standard deviation for total accuracy, sensitivity, and specificity are reported.

Chapter 4: Results

Random Forest Classification results

Random forest successfully classified individuals as having ASD or not

RF model accuracy is shown in Figure 2A. Applying the RF algorithm on behavioral data from 7 different tasks (34 variables) achieved an overall classification accuracy of 73% (M = .727, SD = .087) and an independent sample t-test revealed that the RF model was significantly more accurate than the permutation accuracy measure of 51% [M = 50.9, SD = .103; t (1998) = 51.325, p < .001]. The RF model

had a sensitivity of 63% (M = .631, SD = .153) when classifying ASD subjects, the ability to correctly identify true positives, and an independent sample t-test revealed that the model's sensitivity was significantly higher compared to the permutation sensitivity of 44%. [M = .441, SD = .166; t (1998) = 26.643, p < .001]. The RF model also had a specificity of 81% (M = .807, SD = .153) when classifying control participants, the ability to correctly identify true negatives, and an independent sample t-test revealed that this was significantly more accurate compared to the permutation specificity of 56%. [M = .564, SD = .153; t (1998) = 40.501, p < .001]. Taken together, these findings show that the RF model identified patterns in the cognitive data that stratified individuals with an ASD diagnosis from individuals without. (Note: Due to confound age and gender factors, a secondary RF analysis was performed on the behavioral data, controlling for both factors. Despite the large confounds, the RF analysis accurately classified ASD from control participants greater than chance. This analysis is discussed in supplemental materials).

Proximity matrices from random forest model suggest subgroups in ASD and Control samples

We next applied community detection to the proximity matrices generated through the random forest modeling. The community detection algorithm identified three putative ASD subgroups and four putative control subgroups (Figure 2B). For children with an ASD diagnosis, the largest subgroup comprised 25 individuals, while the other two subgroups numbered 13 and 9 children respectively. For children without an ASD diagnosis, the largest subgroup comprised 39 individuals; three other subgroups were evenly split with five, five, and three children respectively. Six controls were not identified as part of any community, which were placed into a fifth "unspecified" subgroup. To characterize these subgroups, we first examined whether accuracy of classification varied between subgroups, and then examined variation in the task measures between the subgroups.

ASD subgroups differed in terms of classification accuracy

We next compared the classification accuracy of individuals within each ASD subgroup to see if specific subgroups may have differentially affected RF model performance (Figure 2C). It also allowed us to validate that these subgroups were indeed systematically different from one another based on the cognitive data used in the RF model.



Figure 2. (A) Plot of accuracy for observed (blue) vs. permuted (red) RF models. Wide bars refer to the 25th/75th percentiles and thinner bars refer to the 2.5th/97.5th percentiles. (B) Sorted proximity matrix, where each row and column represents a participant and each cell represents the number of times two participants ended in the same terminal node across all the RF models. (C) Plot of RF classification accuracy for ASD subgroups, error bars represent 1 standard error of the mean (SE). Dashed blue line represents 50% mean accuracy. (D) Plot of RF classification accuracy for ASD subgroups. The color code for each subgroup is maintained throughout all subfigures.

Because we constructed multiple RFs, each subject was included in the test dataset a large number of times, therefore we can calculate the rate of accurate classification per subject. A one-way between subjects ANOVA was conducted to compare the rate of classification accuracy between the 3 ASD subgroups identified by community detection. There was no significant difference between the groups [F (2, 44) =1.859, p=.168]. An independent sample t-test was conducted to see if subgroup classification accuracy significantly differed from chance (.5) using a Bonferroni adjusted alpha level of .0167 per test (.05/3). Subgroup 1 was significantly better at classification than chance [M = .726 SD = .367; t (24) =3.0732, p=.005] but subgroups 2 [M = .607 SD = .383; t (12) =1.01, p=.334] and subgroup 3 [M = .443 SD = .431; t (8) =-.399, p=.701] were not.

These results suggest that there may be differences in our subgroups that are important for distinguishing ASD from TD. This difference is subtle, because effects of subgroup on accuracy are small and could largely be driven by the small sample size in subgroups 2 and 3. However, variation in classification accuracy may reflect differences in cognitive profiles. Subjects in subgroup 3 had a classification accuracy of only 44%, which may indicate that these individuals had cognitive scores more similar to our control group than our ASD group, while subgroup 1 had a classification accuracy of nearly 73% suggesting that their cognitive scores may be far different from both our control group, and ASD subgroup 3.

Control subgroups differed in terms of classification accuracy

We also compared the classification accuracy of individuals within each control subgroup to again see if specific subgroups were differentially affecting our RF model's performance (Figure 2D).

A one-way between subjects ANOVA was conducted to compare classification accuracy for each of the 4 control subgroups plus the controls that were lumped into a fifth subgroup, identified by community detection. There was a significant effect of subgroups on classification accuracy [F (4, 53) =24.018, p<.001]. Post-hoc comparisons using an independent-sample t-test indicated that the classification accuracy for subgroup 5 (M = .120 SD=.086) was significantly worse (using a Bonferroni adjusted alpha level of .006 per test) than subgroup 1 [M = .922 SD = .137; t(43)=-13.871, p<.001], subgroup 2 [M = .804 SD = .422; t(9)=-3.910, p=.004], and subgroup 4 [M = .995 SD = .0089; t(7)=-16.903, p<.001], but not subgroup 3 [M = .636 SD = .362; t(9)=-3.411, p=.008]. Additionally, an independent sample t-test was conducted to see if subgroup classification accuracy significantly differed from chance (.5) using the Bonferroni adjusted alpha level of .006 per test. Participants in subgroups 1 [t (38) =19.276, p<.001] and 4 [t (2) =96.00, p<.001] were classified as controls significantly more than chance, while participants in subgroup 5 [t (5) =-10.773, p<.001] were classified as controls significantly less than chance.

Community Detection identified these subgroups in ASD and Control samples who differed in behavioral tasks and classification accuracy

To test whether ASD subgroups may reflect quantitative variation in autism symptom severity, we examined whether identified ASD subgroups varied by Social Responsiveness Scale (SRS). A one-way ANOVA revealed no significant differences between the subgroups on SRS (Figure 2E; F (2, 44) = 0.006, p



= 0.994), suggesting that ASD subgroups had similar autism severity but varied in other ways. Because normal variation in cognitive profiles may affect the manifestation of a developmental disorder (71), we then examined the variation in task performance for ASD (Figure 3; left) and

Figure 3. Radar plots represent the 50th percentile for performance per group. All data are normalized within each radar plot from 0 to 100 percent. Per sample, one-way ANOVAs were conducted on raw data to reduce the number of points plotted based on differences between subgroups. The colors for each subgroup are the same as in Figure 2.

control (Figure 3; right) subgroups. For control subgroups, the fourth subgroup was not examined due to the small sample size and the fifth subgroup was not examined because it represented "unspecified" subjects. A series of subgroupXtask measure repeated measures ANOVA were performed to assess whether we should examine task performance between specific subgroups. The ASD subgroups (F(66,1056) = 7.65, p = $7.5*10^{-54}$), control subgroups (F(66,1452) = 2.19, p = $2.4*10^{-7}$), and accurately identified subgroups (F(33,1716) = 10.64, p = $3.3*10^{-49}$) showed significant differences across task, indicating that identified subgroups varied by task measure. Post-hoc one-way ANOVAs identified 11 significant different features for control subgroups (F (2, 46) > 3.29, p < 0.0462) and 16 significant

different features for ASD subgroups (F (2, 44) > 3.45, p < 0.0405). For both ASD and control subgroups, similar relative cognitive profiles were observed. The largest subgroup in both cohorts performed best on stop and continuous performance tasks. The second largest subgroup in both cohorts had the smallest spatial span, and the highest accuracy and longest reaction times for the facial and affect processing tasks. The third subgroup in both cohorts was characterized by highest spatial span, but lowest accuracy and shortest reaction time for the face processing tasks. Participants who show a combination of low accuracy and short reaction time may be showing a speed accuracy trade-off (90), where individual participants are making quicker responses at a cost of more accurate responses. For the most part, delayed discounting did not differentiate the subgroups, which is unsurprising, because evidence is mixed whether delayed discounting varies by ASD or ASD subgroups. A prior study suggests that ASD and control subgroups discount monetary rewards similarly(24); the relationship between discounting and time varies by ASD subgroup, which is consistent with findings from a separate study where some ASD participants may discount monetary rewards more steeply than controls(25). The similar cognitive profiles observed between controls and ASD subgroups suggests that normal variation in cognitive profiles may impact how ASD manifests in individuals.

AUD 24 CIO 40 DOA 32 FRP 24 RET 8 SMM 88 SAL 4 VEA 23 VIS 39 SBOT 19 NON 47

Functional Connectivity Results

Figure 4. Visualization of systems of the brain used in the chi-squared analysis. Aud = Auditory. CIO = Cinguloopercular. CIP = Cingulo-parietal. Def = Default-mode. DoA = Dorsal attention. FrP = Frontal-parietal. ReT = Retrosplenial. SMh = Somato-motor hand. Smm = somato-motor mouth. VeA = ventral attention. Vis = Visual. SBcT = subcortical. Non = none.



Functional connectivity differences between ASDs and Controls

To test our hypothesis that our ASD and controls groups differed in terms of resting-state functional connections between, and within, different functional systems, we used the chi-squared approach described earlier. The Gordon parcellation plus 19 subcortical regions were used to define the modules (Figure 4). We conducted the analysis on the 26 ASD subjects



Figure 5. (A) Plot of t-statistics for significant clustering observed between ASD and controls. (B) Plot of F ratios for significant clustering observed in the ANOVAs by subgroup. Colors surrounding significant clusters reflect the functional systems involved in the module (e.g. within or between system connectivity). (C) Visualization of estimated marginal means via subgroup by network interactions. Error bars represent 2 times the standard error of the mean. Colors surrounding the boxes reflect the functional systems involved and are consistent with the colors in B.

and 42 control subjects with satisfactory fMRI data (Figure 5A). The chi-squared analysis revealed significant clustering effects between the cingulo-opercular system and the default mode system (χ 2 = 48.86, p =.0002), the somato-motor hand system and the default mode system (χ 2 = 12.81, p =.0016), the visual system and default mode system (χ 2 = 11.74, p =.001), and between the subcortical system and the dorsal attention system (χ 2 = 35.05, p =.0024). It also revealed significant clustering effects within the cingulo-opercular (χ 2 = 259.36, p =.0002), the default mode system (χ 2 = 11.66, p =.0002), and the visual system (χ 2 = 35.05, p =.0002). These findings are consistent with prior reports of rsfcMRI differences between TD and ASD samples (see: Discussion).

	Table of marginal means from chi-square test			
Module	control SG1	ASD SG1	ASD SG2	ASD SG3
AUD-CIP	-0.04 (0.004)	0.12 (0.01)	-0.02 (0.01)	-0.04 (0.009)
CIO-DEF	-0.09 (0.002)	-0.09 (0.005)	-0.02 (0.005)	-0.02 (0.004)
DEF-DEF	0.17 (0.002)	0.09 (0.005)	0.13 (0.005)	0.1 (0.005)
DEF-SMH	-0.02 (0.002)	-0.037 (0.005)	-0.06 (0.005)	-0.002 (0.003)
DOA-SMH	-0.005 (0.002)	-0.004 (0.006)	0.04 (0.006)	0.03 (0.004)
DOA-SBCT	-0.02 (0.002)	-0.06 (0.008)	-0.07 (0.007)	-0.05 (0.005)
SAL-VIS	-0.04 (0.004)	0.05 (0.01)	0.03 (0.01)	-0.03 (0.008)

Table 4. A list of the estimated marginal means from the chisquare ANOVA test. Values in parentheses reflect the standard error of the marginal means.

Subgroup differences within ASD and control samples

Because ASD subgroups differed in classification accuracy with respect to chance (Figure 2C), we also tested whether variance between each of the ASD subgroups and the large control subgroup differed in terms of resting-state functional connections between, and within, different function systems, using the chi-squared analysis. Unfortunately, due to the MRI 'scrubbing' procedure, we did not have sufficient data in the

other control subgroups to include them in this analysis. We conducted a one-way ANOVA with four groups on 57 subjects: the 31 subjects from Control subgroup one, 12 subjects from ASD subgroup 1, 8 subjects from ASD subgroup two, and 6 subjects from ASD subgroup three who had satisfactory fMRI data. We again used a permutation test to determine each system's expected ratio and compared this to the observed ratio using the chi-squared analysis (Figure 5B). We used the estimated marginal means from the ANOVA to visualize which subgroups drove significant clustering (Figure 5C). This test revealed significant increases in connectivity for ASD subgroup 1, relative to all other subgroups, between the cingulo-parietal system and the auditory system ($\chi 2 = 12.06$, p = .0014). Significant increases in ASD subgroup 2 and 3 between the cingulo-opercular system and the default system ($\chi 2 = 24.01$, p = .0002), and between the dorsal attention system and the somato-motor hand system ($\chi 2 = 15.37$, p = .0006). Significant increases in ASD subgroup 1 and 2 connectivity between the salience system and the visual system ($\chi 2 = 11.36$, p = .0016). Significant increases in control connectivity were observed within the default system ($\chi 2 = 22.36$, p = .0010) and between the dorsal attention system and the subcortical system ($\chi 2 = 11.85$, p = .002). Connectivity between the default system and the somato-motor hand system (χ^2 = 28.85, p = .0002) showed mixed results, with ASD subgroups deviating from controls. The estimated marginal means for these tests are summarized in Table 4.

These differences overlapped substantially with the differences observed between ASD and controls (Figure 5A), suggesting that normal variation in mechanisms that are also affected by ASD may cause variation in how ASD may manifest (1,91). These findings should be interpreted cautiously, however, because these data are not predictive of diagnosis.

Supplemental analysis 1: Age and gender are not associated with most input features

Supplemental figure 1 shows the relationships observed between age (Figure 6;blue), gender (Figure 6; red), and task measures. No measure was significantly associated with gender, after correction for multiple comparisons ($R^2 < 0.045$, p > 0.169). However, eight features were significantly correlated with



0.001), spatial

matches other radar plots in figure 3 and Figure 8.

span backward RT ($R^2 = 0.105$, p = 0.001), spatial span forward span ($R^2 = 0.086$, p = 0.002), spatial span forward number completed ($R^2 = 0.077$, p = 0.004), and accuracy on stop go trials ($R^2 = 0.165$, p < 0.001). Despite this relationship, measures that show insignificant correlations with age, such as stop signal RT $(R^2 = 0.022, p = 0.136)$, standard deviation of stop go trial RT ($R^2 = 0.026, p = 0.099$), facial affect accuracy ($R^2 = 0.045$, p = 0.033), and auditory affect RT ($R^2 = 0.039$, p = 0.049), strongly characterized the differences between subgroups (Figure 3) and between diagnostic samples (Figure 9). This analysis suggests that gender and age may have had minimal influence on the predictive features despite the differences between ASD and TDs.

Supplemental analysis 2: RF classified ASD diagnosis and identified three ASD subgroups and two control subgroups





Figure 7. (A) Plot of accuracy for observed (blue) vs. permuted (red) RF models after controlling for age and gender. Wide bars refer to the 25th/75th percentiles and thinner bars refer to the 2.5th/97.5th percentiles. (B) Sorted proximity matrix, where each row and column represents a participant and each cell represents the number of times two participants ended in the same terminal node across all the RF models. (C) Plot of RF classification accuracy for ASD subgroups, error bars represent 1 standard error of the mean (SE). Dashed blue line represents 50% mean accuracy. (D) Plot of RF classification accuracy for TD subgroups. Error bars represent 1 SE. Dashed blue line represents 50% mean accuracy. (E) Plot of SRS for ASD subgroups. The color code for each subgroup is maintained throughout all subfigures.

RF model accuracy is shown in supplemental figure 2A. Applying the RF algorithm on behavioral data from 7 different tasks (34 variables) achieved an overall classification accuracy of 62% (M = .623, SD = .063) and an independent sample t-test revealed that the RF model was significantly more accurate than the permutation accuracy measure of 50% [M = .504, SD =.077; t(1998) = 37.83, p < .001]. The RF model had a sensitivity of 64% (M = .647, SD = .123) when classifying ASD participants, the ability to correctly identify true positives, and an independent sample t-test revealed that the model's sensitivity was marginally, albeit significantly, higher compared to the permutation sensitivity of 47%. [M = .467, SD =.137; t(1998) = 30.98, p < .001]. The RF model also had a specificity of 60% (M = .603, SD = .106) when classifying TD participants, the ability to correctly identify true negatives, and an independent sample ttest revealed that this was significantly more accurate compared to the permutation specificity of 53%. [M = .534, SD =.123; t(1998) = 13.55, p < .001]. After controlling for age and gender, the RF model separates TDs and ASDs equally. However, the proximity matrix notes strong separation between the groups (Figure 2B). Because few predictive features were significantly related to age and gender, but age and gender were significantly different between the cohorts, the observed loss of accuracy may reflect increased noise in the residuals as opposed to a removal of age and gender confounds.

Proximity matrices from random forest model suggest three subgroups each for ASD and two for control cohorts

The community detection algorithm identified three putative ASD subgroups and two putative TD subgroups (Figure 7B). For children with an ASD diagnosis, the largest subgroup comprised 27 individuals, while the other two subgroups numbered 15 and 4 children respectively. One child was not part of any community and left out of remaining analyses. For children without an ASD diagnosis, the largest subgroup comprised 31 individuals, the second group numbered 27 individuals. To characterize these subgroups, we first examined whether accuracy of classification varied between subgroups, and then examined variation in the task measures between the subgroups.

ASD subgroups differed in terms of classification accuracy

A one-way between participants ANOVA was conducted to compare classification accuracy between the 3 ASD subgroups identified by community detection (Figure 7C). There was a significant effect of subgroups on classification accuracy [F(2,43) = 12.212, p<.001]. Post-hoc comparisons using an independent-sample t-test indicated that the classification accuracy for Subgroup 3 (M = .005, SD = .007) was significantly worse than Subgroup 1 [M = .706, SD = .297; t(27) = -4.645, p < .001] and Subgroup 2 [M = ..678, SD = .237; t(17) = -5.558, p < .001], while Subgroups 1 and 2 were not significantly different from one another [t(40) = .315, p = .754].

An independent sample t-test was conducted to see if subgroup classification accuracy significantly differed from chance (.5) using a Bonferroni adjusted alpha level of.017 per test (.05/3). Subgroup 1 [t(26) = 3.604, p = .001] and Subgroup 2 [t(14) = 2.908, p = .012] were both significantly better at classification than chance, while Subgroup 3 was significantly worse than chance [t(3) = -146.247, p < .001].

TD subgroups differed in terms of classification accuracy

Supplemental figure 2D shows the accuracy for TD subgroups. An independent samples t-test was conducted to compare classification accuracy between the two TD subgroups identified by community detection which revealed that Subgroup 1 (M = .870, SD = .286) had significantly higher classification accuracy compared to Subgroup 2[M = .287, SD = .240; t(56) = 8.339, p < .001].

An independent sample t-test was conducted to see if subgroup classification accuracy significantly differed from chance (.5) using the Bonferroni adjusted alpha level of .025 per test (.05/2). Participants in Subgroups 1[t(30) = 7.206, p < .001] were correctly classified as TDs significantly more than chance, while participants in Subgroup 2 [t(26) = -.4.611, p < .001] were incorrectly classified as ASD more than chance.

Similar cognitive profiles were identified with ASD and within TD subgroups

To test whether ASD subgroups may reflect quantitative variation in autism symptom severity, we examined whether identified ASD subgroups varied by Social Responsiveness Scale (SRS; Figure 7E). A one-way ANOVA revealed no significant differences between the subgroups on SRS (F(2,44) = .012, p = .012,



suggesting that ASD subgroups may have had similar autism severity but varied in other ways.

.988),

Because normal variation in cognitive profiles may affect the manifestation of



a developmental disorder (Fair, 2012), we then examined the variation in task performance for ASD (Figure 8; left) and TD (Figure 8; right) subgroups. For both sets of subgroups, all measures were significantly different. For both ASD and TD subgroups, similar cognitive profiles were observed and separated by overall task performance. The largest subgroup performed best across all tasks. The second largest subgroup performed worst across all tasks. For ASD, the third subgroup was characterized by varying performance in the middle.

Supplemental Analysis 3: Subgroups did not vary by ADOS scores

ADOS symptoms for the original (Figure 9A) and supplemental (Figure 9B) subgroups are shown in Figure 9. For the original analysis, no significant effects of subgroup were observed (F(2,46) = 1.122, p = 0.335),



Figure 9. Bar plot of ADOS summed scaled scores for ASD subgroups. Error bars reflect one standard error of the mean. Subgroups are color-coded by their affiliated colors (see: Figure 2). (A) ADOS summed scaled scores for original subgroups. (B) ADOS summed scaled scores for supplemental subgroups.

affected by demographics, particularly differences in gender.

and the largest numerical difference was observed between the first (M = 11.8 SD = 2.79) and second (M = 13.54 SD = 3.52) subgroups (cohen's d = 0.53). For the supplemental analysis, no significant effects of subgroup were observed (F(2,45) = 1.256,p = 0.295). However, large numerical effects were observed comparing the third subgroup (M = 10.75 SD = 1.258) to the first (M = 12.07 SD = 3.234 ; cohen's d = 0.56) and second (M = 13.4 SD = 3.924 ; cohen's d = 0.9) subgroups. The large effect size in the supplemental results may have been

Supplemental Analysis 4: Supplemental subgroups varied by age and gender; original subgroups varied by age

Therefore, we examined whether the ASD and TD subgroups varied by age (Figure 10), gender and IQ



Figure 10. Bar plots of age for original (top) and supplemental (bottom) subgroups. Plots are split by ASD (left) and TD (right) subgroups. Error bars reflect one standard error of the mean. Subgroups are color-coded by their affiliated colors (see: Figure 2). (A) Age for original ASD subgroups. (B) Age for original TD subgroups (C) Age for supplemental ASD subgroups (D) Age for supplemental control subgroups.

(Figure 11). For the TD original subgroups, we found no significant variation in age (Figure 10B; F(4,57) = 2.09, p = 0.095), IQ (Figure 11B; F(4,57) = 2.33, p =0.068), or gender $(\chi 2(df = 4, N = 57) =$ 4.979, p = 0.290). The supplemental subgroups split into female (first) and male (second) subgroups ($\chi^2(df =$ 1, N = 57)= 58.00, p <.001) but showed no significant age (Figure 10D; t(56) =0.343, p = 0.733) or

IQ (Figure 11D; t(56) = -1.54, p = 0.129) differences, suggesting that the supplemental RF may have classified the groups primarily on gender differences.

Both the ASD supplemental and original subgroups varied by age (Figure 10) and IQ (Figure 11), but in very different ways. For the original subgroups, the largest (N = 25) and best classified subgroup had significantly lower age (Figure 10A ; F(2,46) = 3.39, p = 0.043) and IQ (Figure 11A ; F(2,46) = 8.4, p = 0.001). For the supplemental subgroups, the smallest (N= 4) and worst classified subgroup had significantly lower age (M = 9.76, SD = 1.59) and IQ (M = 24.3, SD = 9.95). We suspect that the discrepancy between the original and supplemental results may be driven by differences in gender composition; the supplemental ASD subgroups varied by gender ($\chi 2$ (df = 2, N = 57) = 20.112, p =<.001), with the smallest subgroup comprising female ASD children, whereas the original ASD subgroups did not vary by gender ($\chi 2$ (df = 2, N = 57) = .875, p = .646).



Figure 11. Bar plots of IQ, as measured by block design scaled scores for original (top) and supplemental (bottom) subgroups. Plots are split by ASD (left) and TD (right) subgroups. Error bars reflect one standard error of the mean. Subgroups are color-coded by their affiliated colors (see: Figure 2). (A) Age for original ASD subgroups. (B) Age for original TD subgroups (C) Age for supplemental ASD subgroups (D) Age for supplemental TD subgroups. Abbreviations: WISC: Wechsler Intellectual Scale for Children; BD: Block Design.



Figure 12. Age (top) and IQ (bottom) bar plots for accurately classified original (left) and supplemental (bottom) subgroups. Error bars reflect one standard error of the mean. Subgroups are color-coded by their affiliated colors (see: Figure 2). (A) Age for original subgroups. (B) Age for supplemental subgroups (C) IQ for original subgroups (D) IQ for supplemental subgroups. Abbreviations: WISC: Wechsler Intellectual Scale for Children; BD: Block Design. Supplemental Analysis 5: accurately classified supplemental, but not original, subgroups differed by age and IQ. Given the uncertainty with the supplemental analysis, we examined whether the results of either analysis could be explained by age or IQ. If successfully classified ASD and typical subgroups vary by demographics, than such variation could

affect the RF model. Therefore, age and IQ were compared using a one-way ANOVA across ASD and TD subgroups that were accurately classified in the original (Figures 2C and 2D) and the supplemental (Figures S2C and S2D) analyses.

IQ and age for accurately classified supplemental and original subgroups are shown in Figure 12. For the original analysis, subgroups did not significantly vary by

age (Figure 12A; F (2,66) = 1.37, p = 0.261), or IQ (Figure 12C; F (2,66) = 2.65, p = 0.078). However, IQ may be numerically lower in the ASD subgroup (M = 34, SD = 12.75) than in the first (M = 40.5, SD = 12.64; cohen's d = 0.51) or fourth (M = 46.3, SD = 9.61; cohen's d = 1.1) TD subgroups. For the supplemental analysis, both age (Figure 12B; F (2,72) = 11.29, p < 0.001) and IQ (Figure 12D; F (2,72) = 3.13, p = 0.05) showed significant variation across the subgroups. In particular, the TD subgroup was numerically younger (M = 10.3, SD = 0.157) and had lower IQ (M = 35.6, SD = 13.7) than the ASD subgroups.

Supplemental Analysis 6: Eight features contributed meaningfully to classification

Supplemental figure 8 shows the variable importance for all 34 features. Only 8 of the 34 features contributed meaningfully to classification: mean stop task RT, standard deviation stop task RT, spatial span backwards RT, spatial span backwards span, spatial span forwards RT, accuracy on face identity task, accuracy on face emotion task, and RT on vocal affect task.

The eight feature RF performed similarly to the original RF. Total accuracy was slightly higher for the original (M = 0.727, SD = 0.087) than the eight feature (M = 0.7144, SD = 0.0577) RF. Sensitivity was higher in the eight feature (M = 0.678, SD = 0.114) than in the original (M = 0.631, SD = 0.153) RF. Specificity was higher in the original (M = 0.807, SD = 0.153) than in the eight feature (M = 0.743, SD = 0.0914) RF.



Figure 13. Plot of variable importance for each feature included in the analysis. The variables are ordered by task, from left to right, in the same order as the radar plots. Positive values indicate that removing the feature from the model increases error (i.e. reduces performance), and therefore are more important variables for the RF model.

relationships between gender and task performance are observed. Second, we performed a second RF model controlling for age and gender across all features, which continued to perform above chance (see: supplemental materials for discussion).

Chapter 5: Discussion Accuracy of the Random Forest

model

Link our results to prior findings using machine learning ASD classification

Using a RF model, ASD and control participants were accurately classified 73 percent of the time using a comprehensive battery of cognitive tasks often identified as affected by an ASD diagnosis. Despite differences in age between samples, it is unlikely that the accurate classification was driven by age for two primary reasons. First, task measures important for classification did not show strong correlations with age (see: supplemental materials for discussion); when corrected for multiple comparisons, no

Higher performance has been reported for behavior when constructing a model using visual face scanning (88.1%; (92)) or goal-oriented reach (96.7%; (93)) measures. However, high classification accuracy may be a function of validation strategies or sample size. Liu et al used a leave-one-outcross validation (LOOCV) strategy, which improves classification accuracy within a test dataset, but may reduce the generalizability of the model to other datasets. Crippa et al. also used a LOOCV validation strategy, and were also limited in sample size. Machine learning approaches using imaging data have shown that validation accuracy decreases as the sample size increases, suggesting that these small sample sizes may be overfitting the data (65,68).

Recent classification studies incorporating brain measures have shown comparable results to our initial classification and further suggest that heterogeneity of clinically relevant ASD subgroups may limit high classification accuracy. Duchesnay et al. found that PET imaging could be used to predict ASD with 88% accuracy in a sample of 26 participants (61). Murdaugh et al. used the intra-DEF connectivity to predict ASD with 96% accuracy in a sample of 27 participants (62). Wang et al., using whole-brain functional connectivity, correctly predicted ASD with 83% accuracy in a sample of 58 participants (63). Jamal et al. used EEG activity during task switching to predict ASD with 95% accuracy in a sample of 24 participants (64). Using large data consortiums like the Autism Brain Imaging Data Exchange (ABIDE), recent classification studies have developed and tested models using datasets with over 100 participants. Collectively, these large-sample studies demonstrate performance accuracy from 59% to 70% when testing untrained data (65–68,94). Our data highlights the importance of considering heterogeneity for such tests.

Extension of prior Machine Learning studies

Individual classification results and their relation to subgroups

Our RF approach extends prior studies by identifying putative subgroups from a validated ASD classification model. Specifically, we identified three ASD and four control putative subgroups, with a fifth group of isolated subjects. To further characterize these subgroups, we examined whether subgroups were stratified via classification accuracy. Because of our extremely stringent inclusion criteria, we are extremely confident that all ASD subjects indeed have an ASD, therefore ASD subgroups that contain misclassified individuals may represent clinically important subgroups that our initial RF model failed to capture. Control subgroups that contain misclassified individuals may represent subgroups that our initial RF model confused for ASD individuals. We found that the largest subgroup for ASD and the largest and smallest subgroup for controls were significantly more accurate than chance. Other ASD and control subgroups were not, and the distinction in classification accuracy may reflect the heterogeneity within the disorder. In an earlier study, ASD participants were sub-grouped on the basis of symptom severity, verbal IQ, and age, which caused classification rates to increase by as much as 10% (65). On the other hand, the fact that control subgroups also showed misclassification suggests that variation in such skills may represent the existence of broad cognitive subgroups that are independent of diagnosis, whose variation may impact the presentation of ASD symptoms (1). Prior work by Fair et al. has shown similar heterogeneity in both TD and ADHD children; as with Katuwal, taking into account this heterogeneity improved diagnostic accuracy (71).

ASD subgroups are not associated with variance in symptom severity

It is controversial whether clinical subgroups even exist in ASD. Recently, it has been suggested that ASD represents the tail end of a continuous distribution of social abilities. Categorically distinct subtypes are

either artificial constructs (95) or unknown (1). Categorically distinct subtypes may be difficult to discover due to the heterogeneity present within the typical population (71) as well as the heterogeneity in genetic causes of ASD (1). According to Constantino et al., such genetic subtypes may interact with the environment of the individual, leading to varying manifestations of ASD. Findings that the trajectories of adaptive functioning and autism symptom severity are distinct from one another (14,91) further suggests a dissociation between adaptive functioning and symptom burden.

Therefore, our subgroups may reflect the variation in autism symptom severity or in cognitive mechanisms that may impact ASD profiles, independent of severity. To test this hypothesis, we examined whether our ASD subgroups varied by autism symptom severity, as measured by the SRS (96) and the ADOS (Supplemental Analysis 3). We found that our subgroups did not differ on the SRS or the ADOS, suggesting that autism symptom severity was similar across the three subgroups, despite differences in classification accuracy. Because we are confident in the ASD diagnosis, we suspect that the variation between these three subgroups reflects typical variation in cognitive mechanisms, which may be independent of autism symptom severity but influence ASD presentation(14,91). Identification of such subgroups may be critical for the development of personalized treatment approaches in future studies and has the potential for improving ASD diagnosis and long term outcomes (1). Future studies could better characterize putatively identified subgroups by examining how subgroups may differ on measures of adaptive functioning, or examining whether the subgroups may be characterized by a set of measured ASD symptoms. Critically, future studies should also seek to assess the stability of identified subgroups using longitudinal data.

Describe identified subgroups

To further characterize the identified subgroups, we examine how the subgroups differed on the tasks incorporated into the model. With such an analysis, we can compare our results to prior research that has identified subgroups in independent datasets using similar tasks (71). Replication of similar subgroups would suggests these subgroups may be meaningful. However, because the data from these tasks were used to construct the model, an independent set of measures is necessary to establish the validity of the identified subgroups. Therefore, we also examined differences in functional brain organization in a subset of participants, to see whether differences in functional brain organization between the subgroups reflects the effect of an ASD diagnosis on functional brain organization.

Differences in behavior and how that compares to previous literature

Due to fragmentation and limited sample size, we examined variation in task performance between the three ASD subgroups and between the largest three control subgroups only. Similar to prior research, subgroup differences were largely similar, independent of clinical diagnosis. Per sample, the largest subgroups performed best on CPT and stop tasks, and worst on face processing tasks. The second largest subgroups had the smallest spatial span and were slower but more accurate on the face processing tasks. The third largest subgroups had the largest spatial span and were faster, but less accurate, on the face processing tasks. The distinctions between these subgroups are consistent with prior research, which characterized heterogeneity in typical and ADHD samples and found multiple subgroups characterized by either a small spatial span, slow RT, and high information processing, or high spatial span, fast RT and low information processing(71). Taken together, these findings suggest that clinical heterogeneity may emerge from normal variation in cognitive profiles, and are consistent with a recent study showing that clinical heterogeneity within ASD may be driven by normative

development(97). Our study here extends the prior findings to ASD and establishes a predictive model, which provides some clinical validity to the identified subgroups.

Our finding that the differences between subgroups were similar in both ASD and TD samples may appear inconsistent with prior studies that show an effect of ASD on the relationship between cognitive measures and task performance(12,27,37,38). However, differences in diagnostic criteria may explain some of the apparent contradiction here. Our study used a team of experts to confirm ASD diagnosis per individual, whereas these prior studies often used only a DSM diagnosis plus one or two instruments that assess autism symptom severity (e.g. the ADOS and/or ADIR). The inconsistency in findings may be interpreted as further evidence of heterogeneity within ASD. Differences in cognitive profiles across individuals with ASD could explain the variation in attention, working memory, and face processing. In addition, prior work suggests that cognitive subtypes within ASD may be similar to cognitive subtypes found in typical populations(98).

Differences in fMRI data and validation of subgroups how that compares to previous literature

To provide further validation of the subgroups, we examined whether significant differences in the functional organization of the brain between subgroups overlapped with significant effects of ASD on functional brain organization. Since this data was never used in the RF model, variation that overlaps with differences between ASD and typical children may reflect clinically or etiologically important distinctions between subgroups. Because we did not observe differences in symptom severity between subgroups, the findings above are more likely to reflect typical variation in neural mechanisms underlying cognitive performance, as opposed to manifestations of ASD symptoms.

Differences between children with and without ASD are consistent with prior studies but also show some novel findings. Children with an ASD have shown altered visual system responses to stacks of oriented lines (99), and at rest they've exhibited altered DEF functional connectivity (52), but not altered cingulo-operuclar connectivity (59). Between system differences have been less studied in ASD, however, sub-cortical cortical connectivity has been shown to be altered (55,57) as well as the dorsal attention network organization (51), which is consistent with altered connections between subcortical and dorsal attention networks. However, differences between the DEF and visual, somatomotor, and cingulo-opercular systems have not been documented. The differences found between somatomotor and DEF may be consistent with findings of altered motor system function in ASD (100), while differences between DEF and cingulo-opercular systems may be consistent with altered rich-club organization (51).

We would like to emphasize that the ANOVA chi-squared analysis may be underpowered (88) and, though enticing, is not definitive. Nevertheless, the subgroup chi-squared ANOVAs hint that the identified subgroups may reflect differences in both mechanisms relevant to an ASD diagnosis, and mechanisms that reflect variation across the subgroups. Four of the seven connectivity modules significantly affected by an ASD diagnosis showed variation in the ANOVA analysis: connectivity within the DEF; connectivity between the DEF and cingulo-opercular systems, between the DEF and somatomotor systems, and between the dorsal attention and subcortical systems. We also found significant variation in the ANOVA chi-squared analysis from the ASD and typical comparisons. Like with behavioral measures in children with and without ADHD, it is possible that variation within the ASD subgroups identified here may actually be "nested" within the normal variation found in brain networks across typical children (1,71,91).

The correspondence between the subgroups and the connectivity profiles are intriguing, and hint that the first ASD subgroup may have altered visual processing mechanisms, the third ASD subgroup may have altered attention mechanisms, and the second ASD subgroup may have both. Speculatively, the first ASD subgroup shows the best ASD performance on both stop and CPT tasks, just as individuals in the first control subgroup performs better than the other control subgroups. Inter-system connectivity between the default mode and task control and attention systems (i.e. CIP and DOA) are control-like in the first ASD subgroup, as well as connectivity between attention and motor systems. As discussed extensively in the introduction, such variation is consistent with the literature and may reflect typical heterogeneity variability related to the presentation of ASD. The third ASD subgroup shows the worst performance on facial and affect tasks of the three ASD subgroups; the first control group performs worse on the same tasks compared to the other control subgroups (Figure 3; right). Such tasks would involve visual processing, and the chi-squared comparison reveals that the third ASD and first control subgroups have similar visual system connectivity. Variation in facial task performance may be implicated in some children with autism (39), but not others (37). It will be interesting to see whether future studies identify similar variation in system-level connectivity between ASD subgroups, and whether these groups are stable over time. In addition, future studies with larger sample sizes may be able to uncover additional or more refined sub-populations within the disorder.

Effects of demographics on RF model performance and subgroup affiliation

Due to the age and gender differences between our ASD and TD samples, we wanted to test whether the typical variation affecting ASD subgroups may reflect differences in demographic variables. We conducted six supplemental analyses (see: Supplemental Materials) to address this question. The analyses detailed extensively in Supplemental Materials are alluded to here. Specifically, we evaluated the effect of age and gender on the behavioral measures (Supplemental Analysis 1), performed the RF classification on behavioral measures when controlling for age and gender (Supplemental Analysis 2), examined the effect of ASD subgroup on ADOS symptom scores (Supplemental Analysis 3), tested whether subgroup affiliation affected age, IQ, or gender (Supplemental Analyses 4 and 5), and measured how much each behavioral measure improved RF classification (Supplemental Analysis 6).

The results from the supplemental RF were concerning, and hinted that controlling for age and gender may have, in fact, biased the analysis in unintended ways. There is some literature(101) that suggests such biases may occur when the differences in groups might differ by the controlling variables, but the features important for classification (i.e. in this case the behavioral measures) are not associated with those variables (i.e., here, age or gender). When we compared the association between age/gender and behavioral measures (Supplemental Analysis 1; Figure 6) to the behavioral measure importance (Supplemental Analysis 6; Figure 13), we found that only a few variables were associated with age or gender; the most important behavioral features showed no association with either demographic variable. After conducting the RF analysis we found several sub-groups that differed primarily by age and gender. Such findings were minimal in the main analysis. The findings provide important context for the primary findings, and highlight the importance of first examining the relationship between nuisance variables and input features. If no associations between input features and regressors are found, but regressors are associated with the outcome variable, then such regression may bias subsequent models in unintended ways. Similar concerns have been found when using parametric tests like analysis of covariance (ANCOVA) in psychiatric research(101). Nonetheless, several considerations arise from these supplementary analyses.

When controlling for age and gender, the supplemental RF (Supplemental Analysis 2) showed a reduction in classification accuracy from 73 to 62 percent (Figure 7A). Nevertheless, the RF model remained significantly above chance for both ASD (64 percent) and TD (60 percent) individuals. Notably, the drop in model performance was driven entirely by the TD group, where performance dropped over 20 percent. Inspection of the subgroups shows that the second TD subgroup was more similar to the ASD subgroups; accuracy for the second TD subgroup was almost zero, suggesting that they were all being classified with ASD (Figure 7D), and therefore ASD classification may be driven by typical heterogeneity. Such an interpretation is consistent with the findings from the original RF. Additionally, We found little evidence that ASD subgroups varied by either SRS (Figure 7E and 2E) or ADOS (Figure 9; Supplemental Analysis 3) measures, which further indicates that ASD subgroups vary by typical heterogeneity and not autism symptom severity. However, it is unclear whether typical heterogeneity reflects demographic variables like age and gender or more cognitive variables like IQ or general task performance (Figure 8). Therefore further analyses investigated what aspects of typical heterogeneity affected subgroup affiliation.

The original RF model may be driven by cognitive profile, while the supplemental RF model may be driven more by demographics

Surprisingly, as noted above, the supplemental RF analysis identified subgroups that varied more by age and gender than the original RF (Supplemental Analysis 4). When we examined variation between control subgroups, we found that the supplemental RF subgroups (Figures S5D and S6D) were split by gender, while the original subgroups showed no demographic differences (Figures S6B and S6D). The ASD supplemental subgroups varied by age (Figure 10C), gender, and IQ (Figure 11C), while the ASD original subgroups varied by age (Figure 10A) and IQ (Figure 11A). The variation in age and IQ differed between the supplemental and original analysis. The most accurately classified ASD subgroup in the original analysis was closest in terms of age and IQ to the control subgroups, while the least accurately classified ASD subgroup in the supplemental analysis was most similar to the control subgroups. Because such demographic differences between accurately classified subgroups may explain the RF classification, we were interested in whether accurately classified ASD subgroups differed from accurately classified control subgroups. Since gender did not vary in the original analysis between ASD subgroups and between control subgroups, we focused on age and IQ variables. We found that age and IQ varied more in the supplemental than in the original analysis, however, IQ was numerically lower in the original ASD subgroup when compared to the control subgroups. Taken together, the findings suggest that the original RF was driven by variation in typical cognitive profiles, whereas the supplemental RF may be affected by variation in gender and age.

Supplemental analysis 1: age and gender are less likely to drive RF classification

Ultimately, we found that the relationship between age and predictive features varied by task. Measures from CPT and spatial span tasks were associated with age, whereas facial affect, delayed discounting, and stop tasks were not. Stop and facial affect tasks contained measures that were considered extremely important by the RF (see: supplemental analysis 6). Taken together, these findings suggest that age and gender are less likely to be driving any RF classification. Nevertheless, it is certainly possible that combinations of variables may be associated with age and gender. Therefore, examining the effects of age and gender on RF classification and subgroup identification can help determine which explanation is more likely.

Supplemental analysis 2: when controlling for age and gender, RF model identifies different subgroups that vary by cognitive profile

RF classification is reduced when controlling for age and gender, but still greater than chance

Compared to the original analysis (Figure 2A), accuracy for the supplemental RF model decreased approximately 11 percent. The reduction in overall accuracy is driven entirely by a 20 percent reduction in specificity, whereas sensitivity was unchanged. Although the reduction in model performance is large, it is difficult to dissociate whether the supplemental or original analysis should be the preferred analysis. Nevertheless, both RFs show over 60% accuracy and perform significantly better than the null models. Therefore, we identified subgroups and examined subgroup similarity and model performance per subgroup.

Two ASD subgroups appear more similar to the second TD subgroup than the third ASD subgroup

In the supplemental RF, model performance varied dramatically by subgroup. The third ASD and second TD subgroups could not be accurately classified, and visual inspection of the similarity matrix reveals almost no similarity between the two TD subgroups, or between the ASD subgroups. In fact, the second TD subgroup was more similar to the first two ASD subgroups than to the other TD group. The supplemental RF subgroups are substantially different from the original RF subgroups, so we further examined how these subgroups may vary by demographics (see: Supplemental Analysis 4 and 5), and cognitive profile.

Subgroups differed by overall performance but not symptom severity

Both ASD and TD subgroups varied by cognitive profile. The third ASD subgroup and first TD subgroup showed high performance across the variables, whereas the second TD and first two ASD subgroups showed low performance. These cognitive profiles are consistent with the model performance; the second TD subgroup and third ASD subgroups could not be accurately classified. Furthermore, autism symptom severity, as measured by the social responsiveness scale, did not vary between ASD subgroups, which suggests that autism symptom severity was similar across the three ASD subgroups. Taken together, these results suggest that the RF model is identifying subgroups by typical heterogeneity rather than ASD symptom severity, which is also consistent with the findings from the original RF.

Supplemental Analysis 3: Effect of subgroup on ADOS scores

ASD original subgroups show no significant variation in ADOS symptom

Both the original and supplemental RF subgroups showed similar effects; we found effect of subgroup on autism symptom severity for either model. Coupled with our prior findings, we are confident that the subgroups identified by both the supplemental and original RFs reflect variation in typical heterogeneity rather than ASD severity. However, typical heterogeneity could reflect variation in demographics, cognitive profile or both. Having already compared cognitive profiles (Figure 3 and Figure 8), we investigated whether demographics such as age, and gender varied within the original and supplemental RF subgroups.

Supplemental Analysis 4: comparison of demographics between ASD subgroups and between TD subgroups

Original ASD subgroups vary by age and IQ

Demographic differences for the original dataset show that age and IQ vary by ASD subgroup, while TD subgroups show no differences in demographics. In particular, the largest and best classified ASD subgroup is both younger and has a lower IQ than the other two ASD subgroups. Notably, this subgroup is closest to the mean age and IQ of the TD subgroups. These findings suggest that the ASD subgroup variation reflects typical variation in cognitive profile, age and IQ, but not gender.

Supplemental ASD and TD subgroups may be driven by gender differences

Demographics differences for the supplemental dataset suggest that TD subgroups were stratified by gender. ASD supplemental subgroups showed significant variation across age, IQ and gender. In particular, the worst classified and smallest subgroup was youngest and had lower IQ. Notably, the poorly classified ASD subgroup shows the greatest demographic similarity to the TD subgroups. TD subgroups were effectively split into male and female subgroups, suggesting that the supplemental RF was driven by gender differences. Given that we controlled for gender, we found this effect somewhat surprising. However, the univariate regression approach does not TD for combinations of multiple variables, which may still enable one to dissociate male from female participants. Therefore, it is unclear whether effects of gender in the supplemental material is artefactual, or represents variation in gender.

Supplemental Analysis 5: comparison of demographics between accurately classified subgroups

Due to small sample sizes, we advise readers to interpret these tests cautiously. Nevertheless, the results here suggest that the RF model in the original analysis does not differentiate between ASD and TD samples by simple age or IQ. In fact, the ASD subgroup closest to the TD subgroups in age shows the highest classification accuracy. IQ shows a numerical difference, suggesting that variation in cognitive profile may have driven the RF. As noted above, subgroups in supplemental appear to be split by gender, but also may vary by both age and IQ. The direction of this variation differs from the original analysis, in that the ASD accurately-classified subgroups are older, more female, have lower IQ, and all of the observed effects are much larger. Taken together with the ADOS and SRS findings, these results suggest that ASD subgroups vary by typical heterogeneity more than autism symptom severity. Notably, the original RF model is less driven by demographic criteria than the regressed model in the supplemental, particularly age. Given that few task variables are associated with age and gender (see: Figure 6), we are concerned that the supplemental regression may have contaminated the analysis. Therefore, we would encourage users to perform such a regression only when an association is observed. Additionally, a careful examination of the subgroup demographics can help determine whether demographics affect the accuracy of the model.

Supplemental Analysis 6: examination of variable importance from features

Variable importance plot shows that eight features contribute to ASD classification. It is noteworthy that none of the eight features show a large relationship with gender or age (Figure 6). Furthermore, features that are controlled by the experimenter, such as accuracy on the stop task, did not contribute meaningfully to classification. All eight of these measures are considered important when evaluating performance on these tasks. On the other hand, both the delayed discounting task and the continuous performance task did not contribute at all to classification. The results from the eight feature RF further suggest that the delayed discounting and continuous performance tasks did not dilute classification.

Chapter 6: Summary and Conclusions

Summary, limitations, and future directions

The current study developed a novel approach for identifying and characterizing putative clinical subgroups and applied the approach to the question of ASD. Putative ASD subgroups identified from a diagnostically validated RF model are more likely to reflect properties relevant to clinical diagnosis than simple examination of the similarity between subjects. Therefore, this approach extends prior work that seeks to cluster and identify clinically important subgroups (71). However, we want to emphasize that the identified subgroups in this sample are putative. To maintain a sensible scope and limit overfitting, we limited the model features to cognitive measures covering executive function and face processing, which do not cover every implicated domain of ASD (6).

To provide more support for the validity of these subgroups, we compared the subgroups using rs-fcMRI data. While we had sufficient power to examine the effect of ASD on resting state data (88), we were underpowered when examining differences between subgroups. Therefore, while the rs-fcMRI analysis provides some evidence that speaks to the validity of the subgroups, the analysis does not fully validate them. In addition, our quality control procedure did not identify enough samples in the 2nd, 3rd, and 4th control subgroups to include them in the rs-fcMRI comparison. Such a comparison would help ascertain how the heterogeneity within and between control and ASD subgroups on behavior relates to rs-fcMRI patterns.

Prior identification of subgroups have relied on calculating the distance between each individual directly (71). Unfortunately, such a method has two primary limitations. First, the diagnosis (or question) of interest is not tied directly to the distance measure. By tying the distance measure directly to diagnosis we can be more confident that the identified subgroups are relevant to the clinical question. Second, the proximity method employed by the RF approach implicitly handles missing data. Using the same dataset, we could not calculate a correlation matrix because we do not have all the data, and excluding participants by missing data would bias the subgroup identification. Nevertheless, we hope future studies will compare our approach with other detection techniques in order to better evaluate the performance.

Validate results and subgroups on external data set

Because we are continuing to acquire data on these and new participants, we will be able to use external data to test whether behaviorally identified subgroups can be predicted from functional connectivity, or structural morphometry data. Furthermore, the approach outlined here can be used in future independent studies to identify putative clinical subgroups acquired at different sites. Ultimately, such independent studies can test whether previously identified subgroups are replicable, and whether such subgroups can be predicted in independent data.

It is important to note that the interpretations of our analyses here are limited by the age and gender gap between the ASD and TD cohorts. Interestingly, we saw no differences of age or IQ across the accurately identified subgroups, nor were any subgroups split by gender. In fact, controlling for age and gender by regressing out these variables, as the supplemental RF model identified subgroups that were strongly affected by age, gender, and IQ. Taken together, these points suggest that the original RF is capturing variation in typical cognitive profile, as opposed to age or gender. Nonetheless, this limitation should not outweigh the novel impact of the approach presented here; future studies can use this RF approach on independent samples and verify whether identified ASD subgroups display similar characteristics to the subgroups identified in the present sample.

With the aid of large-scale data consortiums (e.g. ABIDE(102)), future studies will and should be able to identify putative subgroups and validate them further in larger samples. New tools will be needed to reduce the large dimensionality of the imaging data, and potential site differences in data quality; however, such resources, which provide imaging data on over 2000 participants across multiple sites, should provide a natural extension to the current work.

Taken together, the findings from the supplemental analyses suggest that ASD subgroups vary by typical heterogeneity. The features important for the model were not strongly associated with age and gender. However, controlling for age and gender altered subgroups and reduced classification accuracy to 62 percent. ASD subgroups did not vary significantly by symptom severity scores, however, ASD subgroups in both original and supplemental analyses varied by age and IQ, but in opposite directions. In the original analysis, the largest and most accurately classified ASD subgroup was youngest and had the lowest IQ; accurately classified TD and ASD subgroups were older and had higher IQs; accurately classified TD and ASD subgroups were older and had higher IQs; accurately classified TD and ASD subgroups were older and had higher IQs; accurately classified by age, IQ, and gender. Based on these analyses we suspect the subgroups identified by the supplemental RF were split by gender, and that the age and gender regression may have contaminated the data. Future studies should be cautious in choosing whether to perform such a regression prior to machine learning, especially if the input features and demographics show small relationships, but demographics and clinical outcomes are highly associated.

Summary of findings from supplemental analysis

Taken together, the findings from the supplemental analyses suggest that ASD subgroups vary by typical heterogeneity. The features important for the model were not strongly associated with age and gender. However, controlling for age and gender altered subgroups and reduced classification accuracy to 62 percent. ASD subgroups did not vary significantly by symptom severity scores, however, ASD subgroups in both original and supplemental analyses varied by age and IQ, but in opposite directions. In the original analysis, the largest and most accurately classified ASD subgroup was youngest and had the lowest IQ; accurately classified TD and ASD subgroups were older and had higher IQs; accurately classified TD and ASD subgroups were older and had higher IQs; accurately classified TD and ASD subgroups were older and had higher IQs; accurately classified by age, IQ, and gender. Based on these analyses we suspect the subgroups identified by the supplemental RF were split by gender, and that the age and gender regression may have contaminated the data. Future studies should be cautious in choosing whether to perform such a regression prior to machine learning, especially if the input features and demographics show small relationships, but demographics and clinical outcomes are highly associated.

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